Vocal Folds Dynamics

Depth-Kymography From 2D to 3D in Voice Diagnostics

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www.demul.net/frits

Version 2

1

First Video-kymography project:

"Voice Diagnostics in a New Perspective"

Goal:

To develop and apply a new type of video-camera to image Vocal Folds and their <u>horizontal</u> positions and movements in patients.

> This (second) project:

To measure <u>vertical</u> positions and movements of vocal folds as well.

- Experimental: develop instrumentation
- Numerical: develop simulation of dynamics
- > Develop method to compare measurements and simulations

Project financed by Dutch Technology Foundation NWO/STW: no. 6633

Publications :

- New Laryngoscope for quantitative high-speed imaging of human vocal folds vibration in the horizontal and vertical direction Nibu A. George, Frits F.M. de Mul, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Journ.Biomed.Optics, 13(6), 064024 (2008)
- Depth Kymography: high-speed calibrated 3D imaging of human vocal fold vibration dynamics Nibu A. George, Frits F.M. de Mul, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Phys.Med.Biol. 53 (2008) 2667-2675
- Depth Kymograhpy of Vocal Fold Vibrations: part II. Simulations and direct comparisons with 3D profile measurements Frits F.M. de Mul, Nibu A. George, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Phys.Med.Biol. 54 (2009) 3955-3977.

References: in these papers.

More details and the simulation program can be downloaded from www.demul.net/frits

Contents:

- → 1. Imaging of the vocal folds
 - 2. 2D Video-kymography
 - 3. 3D (Depth-) kymography
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 - 5. Comparison of measurements and numerical results
 - 6. Conclusions

Vocal Folds: top view



1,2: Right and left vocal fold

3: Blood vessel

4: Glottis: opening between folds, partly or completely closed during phonation

Imaged line in Videokymography

Vocal folds: top view

Stroboscopic image



Model: Vocal folds consist of 2 x 2 masses: left/right and upper/lower

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Vocal Folds: top view



2D-Videokymography system



2D-Videokymography system



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Videokymography system with 3D-extension



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Videokymography system with 3D-extension



Videokymography system with 3D-extension





Resolution: 50 µm (hor. & vert.)

Videokymography system with 3D-extension

System characteristics:

Laser: 658 nm, 90 mW (on vocal folds: 14 mW)

Laser line on vocal folds : 18 mm x 0.4 mm

Triangulation angle : 7 °

Camera systems: (may be combined using filtering)

- High-speed camera (Wolf)
 4000 fps, color, 256 x 256 pixels @ 13 x 13 μm²
- Position-sensitive linear detector array (Hamamatsu)
 256 x 2 pixels @ 13 μm x 1 mm.



time

Vocal Folds Dynamics

one cycle

Left: Modal

Right: Falsetto

At left side of each: Dotted region: solid lip Open region: mucosal lip

From: Hirano (1968)

"Conventional" 2D - Kymography

Top view - imaged line as f (time)



tippe

What do we want to see?



2D Kymography line with extra: vertical profile.

Example of results:



Vocal folds with laser line image





Movie: what do we want to see?





2D Kymography line with extra: vertical profile.

Results:





IOP PUBLISHING

Phys. Med. Biol. 53 (2008) 2667-2675

PHYSICS IN MEDICINE AND BIOLOGY

doi:10.1088/0031-9155/53/10/015

Depth-kymography: high-speed calibrated 3D imaging of human vocal fold vibration dynamics

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Abstract

We designed and developed a laser line-triangulation endoscope compatible with any standard high-speed camera for a complete three-dimensional profiling of human vocal fold vibration dynamics. With this novel device we are able to measure absolute values of vertical and horizontal vibration amplitudes, length and width of vocal folds as well as the opening and closing velocities from a single *in vivo* measurement. We have studied, for the first time, the generation and propagation of mucosal waves by locating the position of its maximum vertical position and the propagation velocity. Precise knowledge about the absolute dimensions of human vocal folds and their vibration parameters has significant importance in clinical diagnosis and treatment as well as in fundamental research in voice. The new device can be used to investigate different kinds of pathological conditions including periodic or aperiodic vibrations. Consequently, the new device has significant importance in investigating vocal fold paralysis and in phonosurgical applications.

(Some figures in this article are in colour only in the electronic version)

Awarded

(for the novelty, significance and potential impact on future research)

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> Numerical simulations:

Vocal Folds Dynamics

- **Goals:**
 - 1. To simulate the **horizontal and vertical motions** of the vocal folds, as functions of time
 - 2. To directly compare measurements and simulations

Modeling:

- Vocal folds modelled as **two masses**,
- With horizontal and vertical freedom,
- Connected by **springs and dampers**,
- Driven by **air pressures**
- Simulate (as functions of time):
 - Coordinates
 - Pressures
 - Flows

- Numerical simulations:
- > Vocal Folds Dynamics
- Most important references:
- Ishizaka, K. and Flanagan, J.L., *Synthesis of voiced sound from a twomass model of the vocal cords*, Bell Syst. Tech. Journ. 51, 1972, 1233-1267.
- Titze, I.R., *The human vocal cords: A mathematical model I+II*, Phonetica, 28, 1973, 129-170.
- Koizumi, T., Taniguchi, S., Hiromitsu, S., *Two-mass models of the vocal cords for natural sounding voice synthesis*, J. Acoust. Soc. Amer. 82, 1987, 1179-1192 + corrections

Side view Top view



time

From: Hirano (1968)





Blocks may also have vertical freedom





Pressure distribution depends on actual positions of vocal fold masses.





also for y $x_{0,}, y_0 = position$ at rest

- linear term (prop. to displacement)
- incl. non-linear term
 - incl. closure term





also for y $x_{0,}, y_0 = position at rest$

- constant term ~ velocity
 - incl. closure term
 - incl. singularity smoothing



Pressure forces

depend on exposed area



x- and *y*-positions, thicknesses *d* and widths *w* will vary. see papers for details.

F = P.A



Pressure distribution depends on actual positions of vocal fold masses.



"Combined Model"

- 6 System coordinate variables + 2 masses: for both masses: *x*- and *y*-positions, thicknesses *d*
- 4 Equations of motion *E* (for *x* and *y*, for both masses):

$$E \equiv \frac{d}{dt} (mv) - \sum F = 0$$

$$E = \frac{dm}{dt}\frac{dx}{dt} + m\frac{d^2x}{dt^2} - \left(F_{springs} + F_{dampers} + F_{pressures}\right) = 0$$

- 2 Additional constraining equations:
 - 1. Conservation of total mass
 - 2. y_1 , y_2 , d_1 and d_2 connected
- => 6 Independent variables



Combined Model

Older models: (see ref.)

- 1. Ishizaka & Flanagan:
 - Only x-dependence
 - Fixed depths (d) and widths (w)
 - Forces not in center-of-masses
- 2. Koizumi:
 - No wall connection for upper mass
 - Forces not in center-of-masses



After: Izhizaka & Flanagan and Titze.

All resistances, compliances and inertias:

expressions describing air flow in tubes as f (length, diameter, density, etc.).

(details: see papers)

Vocal tract: components dependent on vowel characteristics (≈ 45 compartments.) **Static situation** (DC): all inertia's (L) = 0 and all compliances (C) = ∞ .



Calculations

(*) Electrical analogon of coupled circuits:
set of 2.(n+2) linear
equations to solve
(n = no. of vocal tract
compartments)

(+) 4 coupled non-linear equations of motion,
with 2 additional constraining equations (total mass, and *y*-positions);
iterative approach.

Input parameters of the simulations

(partly following Ishizaka/Flanigan, Titze, Koizumi, and others).

parameter	parameter
general:	mass 2 : m20 : mass in rest [g]
rhoA: air density [g/cm^3]	: d20 : depth in rest [cm]
lambda: heat conduction coeff [W/(mK)]	: x20 : x-pos in rest [cm]
Cp: specific heat const.press [J/(kg.K)]	: k2x : spring const x [N/m]
eta: adiabatic const [-]	: eta2x: non-lin spring const x [1/cm^2]
c: sound velocity [m/s]	: h2x : collision spring const x [N/m]
mu: air viscosity [Pa.s]or[Ns/m^2]	: etah2x: non-lin coll. const x [1/cm^2]
rhoT: tissue density [g/cm^3]	: zeta2x: damping ratio x [-]
lg : glottis length [cm]	
	coupling : kcx : spring const x [N/m]
mass 1: m10 : mass in rest [g]	: kcy : spring const y [N/m]
: d10 : depth in rest [cm]	: etacx: non-lin spring const x [1/cm^2]
: x10 : x-pos in rest [cm]	: etacy: non-lin spring const y [1/cm^2]
: y10 : y-pos in rest [cm]	: zetacx: damping ratio x [-]
: k1x : spring const x [N/m]	: zetacy: damping ratio y [-]
: k1y : spring const y [N/m]	
: eta1x: non-lin spring const x [1/cm^2]	lungs: Plungs: pressure [Pa]
: eta1y: non-lin spring const y [1/cm^2]	: Rlungs: resistance [kg/(m^4.s)]
: h1x : collision spring const x [N/m]	trachea: length [cm]
: etah1x: non-lin coll. const x [1/cm^2]	: area [cm^2]
: zeta1x: damping ratio x [-]	contraction: length [cm]
: zeta1y: damping ratio y [-]	: area at entrance [cm^2]
	: area at mid point [cm ²]
	: area at exit [cm ²]
	mouth: area [cm^2]

🕼 Vocal Fold	ls Dynamics	: INPUT SCR	EEN											_	
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					(Precalculation	DC-values	j j	3. Combined		41: x M1: v
INPUT DATA	of PARAME	TERS (ed	lit/chan	ge valu	es in	table cells di	rectly; see H	ELP)		M1 (low) width [cm]	0.309) 4. Id+const.volume		41: d
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2 lambda: h	neat conductio	n coeff IW/(n	nK)]	0.026	24	: k2x : spr	ina const x [N/n	n]	15	M2 (up) width [cm]	0.305	8	1. w and d var.		M2: d
3 Cp: specif	fic heat const.	.press []/(ka.l	K)]	1005	25	; eta2x; n	on-lin sprina cor	- nst x [1/cm^2]	100	M2: area [cm^2]	0.056	8	3. w and d const.		PI
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7 rhoT: tiss	ue density [a	/cm^3]		1.04	29	coupling: kcx :	spring const x	[N/m]	15	Plungs [Pa]	1.000E+03		3. w and d const.		22
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Output variables of the simulations

variable (o)	Variable (o)
Model code (*)	DC-flow [lit/s]
Lower mass: $+/-dm1$ [g]	Mouth pressure: $\langle MP \rangle + /- dMP$ [Pa]
$: < x_1 > +/- dx_1 \text{ [mm]}$: flow: $\langle MF \rangle + /-dMF$ [lit/s]
$: < y_1 > +/- dy_1$	Frequencies: 1 st peak [Hz]
\dots : ratio $dy1/dx1$: ratio 2 nd /1 st , 3 rd /1 st , 4 th /1 st , 5 th /1 st peak intensity
: < d1 > +/- dd1	Glottis: closure situation [%]
: < w1 > +/- dw1	: phase delay upper vs. lower mass [degr.]
Upper mass: $< m2 > +/- dm2$ [g]	: averaged duration of open period [ms]
$: < x^{2} + - dx^{2}$ [mm]	: max. open width [mm]
: < y2 > +/- dy2	\dots : max open area [mm ²]
\dots : ratio $dy2/dx2$	
: < d2 > +/- dd2	(o) Notation: for variable x: $\langle x \rangle$ = time average;
$: < w^2 > +/- dw^2$	dx = amplitude of vibration

(*) **Model code:** "ABC" :

A = 1, 2, 3 : model: according to (1) Ishizaka-Flanagan, (2) Koizumi and

(3, present) Combined model respectively;

B = 1: lower mass: both width w and thickness d variable; folds constrained at wall side;

2 : id.: width constant, thickness variable;

3 : id.: width and thickness constant;

C = 1, 2, 3 : **upper mass**, as with B (for lower mass)

Vocal Folds Dynamics : CALCULATION SCREEN





VFDyn-program



Compare: Stroboscopic movie



Some results of the simulations:

- Masses (averages, amplitudes)
- Coordinates (averages, amplitudes)
- Flows, pressures and frequencies
- Frequency peaks: intensity ratios
- Vocal Tract Area Functions
- Frequencies in mouth and glottis
- Comparison of measured and calculated values
- Slope values: (dy/dp) with y = variable (m, x, y, f...) p = parameter $(m_0.x_0, ..., k.s, ...$compartment lengths etc.)

Models: (code ABC)

- 2: Koizumi
- 3: Combined
- B: lower mass
- C: upper mass

e.g. **code 313** : A=3: "Combined model",

- B=1: lower mass: *d* and *w* variable
- C=3: upper mass: *d* and *w* fixed.

Masses (averages, amplitudes) in various models



amplitudes of oscillations

B=1: lower mass: d and w variable C=3: upper mass: *d* and *w* fixed.

Coordinates (averages, amplitudes) in various models



oscillation amplitudes







Frequency peaks: intensity ratios in various models



Models: (ABC) A = 1: Ishizaka/Flanagan, 2: Koizumi, 3: Combined B: lower mass; C: upper mass B,C = 1: d and w var.; 2: d var., w fixed; 3: d and w fixed

Effects of different Vocal Tract Area Functions (VTAF's).



Vocal Tract Area Functions according to Story & Titze. Component length: 0.40 cm.

Effects of different Vocal Tract Area Functions (VTAF's).



Model 312.

The variable values are relative to the values of VTAF = /O!/ (green line). /a:/ has stronger overtones than /i:/ and /O:/.

Effects of different Vocal Tract Area Functions (VTAF's).

/0:/

Vowels /i:/, /o:/, /a:/ (for components: ref. Story & Titze).

Flow in mouth (time) /i:/



Pressure in mouth (gray) and glottis (purple; shifted over 1/20 scale) (freq.)







/a:/

Effects of different Vocal Tract Area Functions (VTAF's). Vowels /i:/, /o:/, /a:/ (for components: ref. Story & Titze).



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Comparison of measurements and simulations



Successive vertical cross sections of the simulations.

Curve: overlay from the corresponding Depth-Kymographic measurement.

Simulation parameter settings adjusted to match measured positions and frequency.

Comparison of measurements and simulations during one vibration cycle



Successive vertical cross sections of the simulations.

Curve: overlay from the corresponding depth-Kymographic measurement.

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Conclusions:

1. Laryngoscope for Depth-Kymography:

- o Design and development are ready
- o Successful tests with human subjects
- 2. The program seems to be capable of simulating the vocal fold dynamics:
 - o In horizontal and vertical directions
 - o With mass exchange between solid mass (lower) and mucosal mass (upper)
- 3. Additional result:
 - Direct comparison between simulations and measurements.

More details and the program can be downloaded from www.demul.net/frits

Publications :

- New Laryngoscope for quantitative high-speed imaging of human vocal folds vibration in the horizontal and vertical direction Nibu A. George, Frits F.M. de Mul, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Journ.Biomed.Optics, 13(6), 064024 (2008)
- Depth Kymography: high-speed calibrated 3D imaging of human vocal fold vibration dynamics Nibu A. George, Frits F.M. de Mul, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Phys.Med.Biol. 53 (2008) 2667-2675
- Depth Kymograhpy of Vocal Fold Vibrations: part II. Simulations and direct comparisons with 3D profile measurements Frits F.M. de Mul, Nibu A. George, Qingjun Qiu, Gerhard Rakhorst and Harm K. Schutte, Phys.Med.Biol. 54 (2009) 3955-3977.

